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Biomechanics

Bite force is limited by the force—length relationship of skeletal muscle in black carp, *Mylopharyngodon piceus*

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Bite force is critical to feeding success, especially in animals that crush strong, brittle foods. Maximum bite force is typically measured as one value per individual, but the force–length relationship of skeletal muscle suggests that each individual should possess a range of gape height-specific, and, therefore, prey size-specific, bite forces. We characterized the influence of prey size on pharyngeal jaw bite force in the snail-eating black carp (*Mylopharyngodon piceus*, family Cyprinidae), using feeding trials on artificial prey that varied independently in size and strength. We then measured jaw-closing muscle lengths *in vivo* for each prey size, and then determined the force–length relationship of the same muscle *in situ* using tetanic stimulations. Maximum bite force was surprisingly high: the largest individual produced nearly 700 N at optimal muscle length. Bite force decreased on large and small prey, which elicited long and short muscle lengths, respectively, demonstrating that the force–length relationship of skeletal muscle results in prey size-specific bite force.

1. Introduction

Durophagous vertebrates (those that eat strong foods like snails or nuts) use high bite forces to counter prey defences. The potential crushing ability of a predator is typically characterized as a single, maximum bite force [1]. This characterization ignores the force–length relationship of vertebrate skeletal muscle: maximum force is produced at intermediate instantaneous muscle lengths and declines when stretched or shortened [2]. Because jaw-closing muscles change length across gapes, bite force should vary with gape size [3]. Whereas bite force is expected to be nonlinear (optimum at intermediate gape sizes), prey force (defensive strength) often increases linearly with size [4,5]. Prey size dictates predator gape during biting, and these different force–size patterns can result in nonlinear predation pressure across prey sizes [6].

Predator bite force can be gape-specific [3,7,8], but general patterns and determinants of gape-specific bite force are not well known. The relationship between predator gape and jaw muscle length has been examined post-mortem [9], but the complex architecture, dynamic moment arms and multiple jaw-closing muscles of many vertebrate feeding systems obscure the relationship between length-specific muscle force and gape-specific bite force.

To link length-specific muscle force with gape-specific bite force in live animals, we explore the pharyngeal jaw apparatus of black carp (*Mylopharyngodon piceus*, a snail-eating fish) as a model system. This model is ideal because it is anatomically and mechanically simple: a single jaw-closing muscle with relatively simple architecture and a static moment arm that elevates the pharyngeal jaw into occlusion. Moreover, the pharyngeal jaws are the only structures in this system capable of mechanical food breakdown. This simple anatomy functionally links length-specific muscle force explicitly to gape-specific bite force.

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Figure 1. Prey strength, prey size and individual success. (*a*) Size and strength (mean \pm 1 s.d.) of manufactured prey items. Grey level reflects tube size. (*b*-*d*) Prey crushing performance by each of the three individuals: 106, 81 and 75 mm head length, respectively. Crushing success spans 100% (black) to 0% (white).

We first test gape-specific crushing performance in black carp using feeding trials with manufactured prey (decoupling prey size from strength) to probe peak bite force across a range of gapes. Second, we use X-ray reconstruction of moving morphology (XROMM) to measure muscle lengths **D**1 used in vivo for each prey size. Third, we characterize the force-length relationship for the same muscles in situ (immediately post-mortem, with the muscle still alive). Finally, we superimpose our in vivo and in situ muscle length measurements to test whether the force-length relationship of the jaw-closing muscle, driven by variable gape in vivo, limits bite performance in a gape-specific way.

2. Material and methods

(a) Specimens

Three farm-raised adult black carp, 650, 550 and 500 mm total length (106, 81 and 75 mm head length), were trained to feed on ceramic tubes filled with pellet food.

(b) Feeding trials

We simulated prey using ceramic tubes from aquarium filter media of four diameters (11.3-16.2 mm). These tubes were selected after surveying available brands for appropriate size (non-gape limiting to our experimental individuals) and accepta-ble strength consistency. We increased strength within each size by coating the tubes in layers of polyurethane (M-coat, Vishay). We tested tube fracture strength using an MTS MiniBionix858 and steel compression platens (jaw-mounted crushing tests could not be aligned consistently) with force directed perpendicu-lar to the long axis of the tube (cineradiography revealed that black carp always crushed tubes in this orientation) and a loading rate of 1 mm s^{-1} . We fractured 5–20 of each prey size/number of coats combination for a total of 317 force-testing trials. We used a 2-way ANOVA with Tukey post hoc corrections to explore differences between specific size/number of coats combinations.

To test feeding performance, we conducted feeding trials with tubes of the same type described above packed with moistened pellet food. Typically, the tube was immediately sucked into the pharyngeal cavity, followed by a crushing attempt. Successful trials involved an audible crack, followed by the fish expelling broken ceramic pieces. We scored the trial unsuccessful if this did not occur within 5 min. We performed less than 10 trials per day with greater than 5 min between trials to avoid satiation and fatigue. Each day, we tested a random mix of the four sizes, proceeding from weak to strong within a size, to probe maximum bite force across sizes. Tests of a given size/ strength combination were discontinued if the first five trials were entirely successful or unsuccessful. Otherwise, five additional tests were conducted.

(c) Radio-opaque marker implantation

Following feeding trials, tantalum spheres (1–2 mm, Bal-Tec) were surgically implanted [10] into the neurocranium and both pharyngeal jaws of anaesthetized animals (MS-222, Argent, 0.05-0.1 g l⁻¹).

(d) Video and force recording

Once normal behaviour resumed, feeding was imaged at 125 fps with biplanar X-ray video (OEC-9400 fluoroscopes, Photron1024PCI cameras) at 80–90 kVp and 20 mA. We analysed 31 feeding trials on 2–3 tube sizes that bracketed the successful crushing range for each individual.

Following *in vivo* data collection, we constructed muscle force–length curves for each individual. Immediately postmortem (Metomidate, 0.1 g l^{-1} followed by cervical dislocation), all musculoskeletal elements were removed from the neurocranium, except for one pharyngeal jaw and its jaw-closing

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127 muscle (m. Levator Arcus Branchialis V; LABV). The preparation was mounted in-series with a force transducer and submerged 128 in oxygenated Ringer's solution (see the electronic supplemen-129 tary material, figure S1). The transducer was anchored to a 130 threaded rod which permitted lengthening between contractions. 131 We endeavoured to orient the jaw in situ in a similar posture to 132 that observed in vivo, and our reconstructions showed a similar 133 position of the muscle insertion site. The muscle was whole-134 field stimulated using a Grass s48H stimulator (10 V, 0.2 ms 135 pulses, 250 pps, 300 ms train) via platinum paddle electrodes to 136 elicit fused tetani. Stimulations started at a short length and 137 successive stimulations (5 min intervals) were completed after 138 1-2 mm lengthening. We continued contractions until force declined below 5 per cent of P_{0} , resulting in 13–20 stimulations/ 139 individual. Because the bilateral muscles can act simultaneously, 140 force was doubled. Imaging was identical to in vivo technique. 141 Herein, we refer to these data as in situ, as they were collected 142 from an electrochemically viable muscle, in its anatomical position, 143 operating in an anatomically relevant way. 144

¹⁴⁶ (e) X-ray reconstruction of moving morphology

We processed X-ray videos using XRAYPROJECT software ([10];
www.xromm.org) and calculated three-dimensional rigid body
movements in MATLAB (The Mathworks). Polygonal mesh
models from laser scans of cleaned bones (Microscan head,
Microscribe MLX articulated arm) were processed in GeoMagic
and re-animated in Autodesk Maya using rigid body movements
from the X-ray videos [11].

We mapped LABV muscle attachment sites onto bone 154 models to measure in vivo and in situ muscle length. We 155 marked origins and insertions of five fascicles with locators in 156 Autodesk Maya, and took straight-line distances between those 157 attachment points. We used the mean of the five distances as a 158 proxy for overall muscle length (in three dimensions) for each 159 time point. We animated the bone models with in vivo data to identify operating lengths during feeding, and in situ data to 160 determine force-length relationships. We used the identical 161 bone model (complete with fascicle positions) for animation of 162 both the *in vivo* and *in situ* data, so that fascicle length measure-163 ments would be directly comparable. Ultimately, only these 164 muscle fascicle length measures were used for further analysis. 165 All data for this study are available at xmaportal.org. 166

3. Results

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The strength of our artificial prey (ceramic tubes) increased with successive polyurethane coatings, although repeated measurements of each size-coat combination showed substantial variability (figure 1*a*). Tube strength varied by tube size and coat number, and these variables interacted significantly (ANOVA, tube type p < 0.001, coat number p < 0.001 and interaction p < 0.001).

177 In vivo prey crushing trials demonstrated decreased crush-178 ing performance (lower success rate) at extreme prey sizes 179 (figure 1) and muscle lengths (figure 2). Tukey-corrected post 180 hoc tests revealed that, for the largest individual, successfully 181 crushed intermediate-sized prey were stronger than larger 182 and smaller prey that were uncrushable (both p < 0.001), indi-183 cating a performance optimum at intermediate prey sizes 184 (figure 1b). Tubes of a given size are effectively larger for smal-185 ler animals, and indeed the two smaller individuals performed 186 optimally on the smallest tubes, and could only crush uncoated 187 13.5 mm tubes (figure $1c_{d}$). Larger tubes (14.4 and 16.2 mm) 188 were uncrushable, regardless of coating, despite the fact that 189 they would fit between the pharyngeal jaws.



Figure 2. Anatomy and performance of black carp pharyngeal jaws. (*a*) Left lateral view of the bones associated with the pharyngeal jaw. (*b*) Lateral view, parasagittal cut-away, showing a schematic of the jaw-closing muscle and individual fibres tracked using XROMM. Note that muscle fibre orientations converge near the bite point, so little or no musculoskeletal leverage amplifies muscle force. (*c*) *In situ* force–length relationships (light grey) and *in vivo* tube-crushing performance (black triangles), normalized to L/L_0 and P/P_0 . Each grey symbol represents a single *in situ* contraction in one individual (head lengths: circle, 106 mm; square, 81 mm; diamond, 75 mm). Up-pointing triangles indicate strongest crushable prey item; *x*-axis error bars denote ± 1 s.d. of *in vivo* muscle lengths, *y*-axis error bars denote ± 1 s.d. of *in vivo* muscle lengths, the strong strength determined via materials testing. All *in vivo* data are pooled in this figure; see electronic supplementary material, figure S1 for *in vivo* muscle length and performance data by individual.

We determined in vivo muscle operating lengths, followed by in situ characterization of the muscle's force-length relationship (figure 2). The jaw-closing muscle of two smaller individuals operated on the descending limb, involving a 50 per cent decrease in peak muscle force (see the electronic supplementary material, figure S1). The largest individual did not operate at similarly long muscle lengths, probably because we could not offer sufficiently large prey to drive its muscle to descending limb lengths. When crushing the smallest prey, the jaw closing muscle of the largest individual operated at ascending limb lengths, corresponding with approximately 50 per cent of P_0 , and bite performance (prey strength) declined to a similar degree. Our threeindividual dataset describes in vivo performance and in situ forces on the ascending limb, descending limb, and plateau regions for the force-length curve, with at least one individual in each region (figure 2c). Our in vivo estimates of bite force fell within 20 per cent of our in situ estimates, and our in situ data always fell within the confidence intervals of the *in vivo* tube strength data (figure 2c).

4. Discussion

Our two independent empirical estimates of gape-specific bite force (*in vivo* maximum-strength tube crushing and

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190 in situ maximally stimulated tetanic muscle force) show that 191 black carp produce high bite forces (350-700 N, electronic 192 supplementary material, figure S1) that vary across gape 193 (figure 2c). By linking these two datasets using identical 194 measures of muscle length from XROMM, we show that 195 length-specific muscle force limits gape-specific bite force.

196 Although the force-length relationship of skeletal muscle 197 has been known for over 70 years [2], it was relatively recently 198 proposed as a factor limiting bite performance [3,8]. All fish in 199 this study voluntarily operated their jaw-closing muscles on 200 the descending limb of their force-length curves, incurring a 201 penalty in muscle force when crushing large prey items 202 (figure 2c). While data from the wild on active selection for 203 prey size are unavailable, we suspect that wild black carp 204 behave similarly.

205 Large size is thought to provide an ecological refuge 206 for prey, due either to the increased strength associated 207 with increased size, or to anatomical constraints on predator 208 mouth opening capability [4-6]. Our study suggests that the ecological refuge for large prey is based not only on increased 210 strength, but also on the requirement of the predator to operate its jaw closing muscles at longer lengths, thus sacrificing 212 muscle force. This could explain why intermediate-sized 213 bivalves experience higher predation pressure than small or 214

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could defensively focus exclusively on getting stronger, exclusively on getting larger or both. Future studies of wild predator-prey interactions could benefit from considering gape-specific bite force. Our study is, to the best of our knowledge, the first relat-

large individuals [6]. This trade-off has ecological ramifications

on prey defence mechanisms and life-history strategies: prey

ing in vivo measurements of bite performance and jaw muscle length to in situ measurements of the force-length relationship for the same muscle. This method allowed us to attribute bite performance as a function of prey size to force production as a function of muscle length. We found that black carp do not possess a single maximum bite force, but rather a range of gape-specific bite forces, shaped by intrinsic muscle properties.

All animal-related procedures were approved by Brown University's IACUC.

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